

Cardiac Rhythm Management Devices (Part I)

Indications, Device Selection, and Function

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PACEMAKER¹ and internal cardioverter-defibrillator (ICD) devices have undergone remarkable evolution since the first implantation of an asynchronous single-chamber pacemaker¹ in 1958 and of an ICD² in 1980. Today, more than 500,000 patients in the United States have pacemakers, and up to 115,000 new devices are implanted each year.³ The number of ICDs implanted each year has steadily increased, reaching 50,000 new implants worldwide in 1999.⁴

Contemporary single- and dual-chamber pacemakers are sophisticated devices, with multiple programmable features, including recently introduced programmable lead configuration^{5,6} and automatic mode-switching.⁷⁻⁹ Many devices use adaptive-rate pacing to modify the pacing rate for changing metabolic needs. First-generation ICDs were short-lived. A formal thoracotomy was required for epicardial lead placement. Today, ICDs are multiprogrammable, are longer-lived, have transvenous leads, and may incorporate all capabilities of contemporary pacemakers.⁴ Furthermore, ICDs have multiple tachycardia detection zones, with programmable detection criteria and tiered therapy (*i.e.*, antitachycardia pacing [ATP], followed by shocks if needed) for each.^{4,10} ICDs also store dysrhythmia event records and treatment results. Finally, clinical experience with an internal atrial cardioverter (atrioverter) has been reported.¹¹⁻¹⁵

In this first installment of a two-part communication, we discuss indications for implanted pacemakers or ICDs, provide an overview of how devices are selected, and describe the basics of device design and function. Only brief mention is made of temporary pacing indica-

tions and technology. In the second installment, we discuss the potential for device malfunction in the hospital environments, perioperative management for patients with implanted devices, and care of patients during device implantation or system revision.

Indications for a Pacemaker or an ICD

Indications for a pacing or ICD device are considered as class I, II, or III.¹⁰ Class I indications are conditions for which there is general agreement that a device may be useful and effective (*i.e.*, is indicated). Class II indications are conditions in which a device is often used but for which there is conflicting evidence or divergence of opinion as to whether it is useful and effective (*i.e.*, may be indicated). Class II indications are subdivided as IIa if the weight of evidence or opinion is in favor of device usefulness or efficacy and IIb if usefulness or efficacy is less well established. Finally, an indication is class III if there is general agreement that a device is unnecessary and possibly even harmful (*i.e.*, not indicated).

Temporary Pacing Indications

Temporary pacing may be required for rate support in patients who experience intermittent hemodynamically disadvantageous bradycardias or for stand-by pacing in patients at increased risk for sudden high-degree atrioventricular (AV) heart block (AVHB). It is also sometimes used to overdrive or terminate atrial or ventricular tachycardias. The endpoint for temporary pacing is resolution of the indication or implantation of a permanent pacemaker for a continuing indication. Transvenous endocardial^{16,17} or epicardial^{16,18} leads are most commonly used for temporary pacing. Noninvasive transcutaneous and esophageal routes are also possible.¹⁹⁻²¹ Transcutaneous pacing produces simultaneous ventricular and atrial capture and thus does not preserve optimal hemodynamics in patients with intact atrioventricular conduction. With available technology for esophageal pacing, only atrial capture is reliable; thus, the method is not suitable for patients with advanced AVHB or atrial fibrillation.

Indications for temporary pacing are not as established as for permanent pacemakers. Usual and less established indications for temporary transvenous or epicardial pacing are listed in table 1.^{18,22-24} AVHB is classified as

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Table 1. Usual and Less Established Indications for Temporary Cardiac Pacing^{18,22-24}

Usual Indications	Less-established Indications
<p>Sinus bradycardia or lower escape rhythms due to reversible cause and with symptoms or hemodynamic compromise</p> <p>As bridge to permanent pacing with advanced 2° or 3° AVHB, regardless of etiology</p> <p>During AMI: asystole; new bifascicular block with 1° AVHB; alternating BBB; symptomatic or disadvantageous bradycardia not responsive to drugs; or type II 2° AVHB</p> <p>Bradycardia-dependent tachydysrhythmias (e.g., torsades de pointes with LQTS)</p>	<p>During AMI: new or age-indeterminate RBBB with LAFB, LPFB or 1° AVHB, or with LBBB; recurrent sinus pauses refractory to atropine; overdrive pacing for incessant VT</p> <p>During AMI: new or age-indeterminate bifascicular block or isolated RBBB</p> <p>Heart surgery:</p> <ul style="list-style-type: none"> To overdrive hemodynamically disadvantageous atrioventricular junctional and ventricular rhythms To terminate reentrant SVT or VT To prevent pause-dependent or bradycardia-dependent tachydysrhythmias <p>During the insertion of a PA catheter in patient with LBBB</p>

AVHB = atrioventricular heart block; AMI = acute myocardial infarction; BBB = bundle branch block; LQTS = long QT interval syndrome, congenital or acquired; RBBB = right bundle branch block; LAFB = left anterior fascicular block; LPFB = left posterior fascicular block; LBBB = left bundle branch block; VT = ventricular tachycardia; SVT = supraventricular tachycardia; PA = pulmonary artery.

first-degree (1°), second-degree (2°), or third-degree (3°; complete) AVHB. Anatomically, it may occur above, within, or below the His bundle.¹⁰ With 1° AVHB, the PR interval is greater than 0.20 s and is usually due to atrioventricular node conduction delay.²⁵ With 2° AVHB, there is gradual PR interval prolongation before dropped beats (type I or Wenckebach 2° AVHB) or no PR interval prolongation (type II or Mobitz 2° AVHB). Type I 2° AVHB is usually associated with a narrow QRS complex, and type II 2° AVHB with a wide QRS complex.¹⁰ In general, type I 2° AVHB with a narrow QRS complex almost always occurs at the atrioventricular node.¹⁰ When associated with bundle-branch block, there is infra-Hisian block in up to 30% of cases.²⁵ Type II 2° AVHB is most commonly encountered when the QRS is prolonged and is generally localized to within the His-Purkinje system.²⁵ Advanced type II 2° AVHB refers to block of two or more consecutive P waves. With 3° AVHB there is no association between atrial and ventricular beats.

Indications for a Permanent Pacemaker

Chronic Atrioventricular Heart Block in Adults.

Patients with atrioventricular conduction abnormalities may be asymptomatic or have symptoms related to bradycardia, ventricular dysrhythmias, or both. The presence or absence of symptoms directly attributable to bradycardia has an important influence on the decision to implant a permanent pacemaker.¹⁰ In addition, many indications for pacing with AVHB have evolved over 30 yr on the basis of experience rather than prospective randomized trials, in part because there is no good alternative treatment.¹⁰

There is little evidence that pacing improves survival with isolated 1° AVHB,²⁶ even though marked 1° AVHB may be symptomatic without higher-degree AVHB.²⁷ This may be because of the close proximity of atrial systole to the preceding ventricular systole.^{28,29} With type I 2° AVHB due to atrioventricular node conduction

delay, progression to more advanced AVHB is unlikely, and pacing is usually not indicated.¹⁰ With type 2° AVHB within or below the His bundle, symptoms are frequent, prognosis is poor, and progression to 3° AVHB is common.¹⁰ Nonrandomized studies strongly suggest that pacing improves survival for patients with 3° AVHB and symptoms.³⁰⁻³⁵ Pacing indications for acquired AVHB are listed in table 2.^{10,22,25}

Chronic Bifascicular and Trifascicular Block. Major fascicles of the conduction system below the His bundle are the right bundle branch and the left anterior and posterior fascicles of the left bundle branch. The latter activate the left ventricular free wall.³⁶ In addition, septal branches of the left bundle branch supply the middle third of the ventricular septum and provide the earliest ventricular activation. Isolated block of any one of these fascicles is unifascicular block. Left or right bundle-branch block with left anterior or posterior fascicular block is bifascicular block. Block involving any three fascicles is trifascicular block.

Electrocardiographic criteria for fascicular block are described elsewhere.³⁶ Syncope is common in patients with bifascicular block but usually is not recurrent or associated with an increased incidence of sudden death.³⁷⁻³⁹ However, bifascicular block with periodic 3° AVHB and syncope is associated with an increased incidence of sudden death.^{40,41} Thus, if the cause of syncope with bifascicular or trifascicular heart block cannot be determined with certainty, or if concurrent drugs may exacerbate AVHB, prophylactic permanent pacing is indicated, especially if syncope may have been due to intermittent 3° AVHB.¹⁰ Although 3° AVHB is most often preceded by bifascicular block, the rate of progression is slow (years). There is no evidence of acute progression to 3° AVHB during anesthesia and surgery.^{42,43} Finally, no one clinical or laboratory variable, including bifascicular block, can identify patients at high risk of death from bradydysrhythmias with bundle-branch block.^{10,44}

Table 2. Indications for Permanent Pacing with Acquired Atrioventricular Heart Block in Adults

Class I—Indicated	Class II—May Be Indicated	Class III—Not Indicated
3° AVHB: Symptomatic bradycardia or need for drugs causing same After catheter ablation of the arterioventricular junction Postoperative and not expected to resolve Neuromuscular diseases Escape rhythm < 40 beats/min or asystole > 3.0 s in an asymptomatic patient 2° AVHB that is permanent or intermittent, with symptomatic bradycardia	Asymptomatic 3° AVHB with average rate > 40 beats/min Type II, 2° AVHB without symptoms (permanent or intermittent) Type I, 2° AVHB at or below His bundle without symptoms 1° AVHB with symptoms of low cardiac output that are relieved by temporary pacing Marked 1° AVHB in a patient with CHF	Asymptomatic 1° AVHB Type I, 2° AVHB above His bundle without symptoms AVHB that is expected to resolve

AVHB = atrioventricular heart block; CHF = congestive heart failure.

Adapted from Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *J Am Coll Cardiol* 1998; 31:1175–209. Copyright 1998 by the American College of Cardiology and the American Heart Association. Permission granted for one-time use. Further reproduction is not permitted without permission of the ACC/AHA.

Pacing indications for chronic bifascicular and trifascicular block are summarized in table 3.^{10,25}

Atrioventricular Heart Block after Acute Myocardial Infarction. Pacing indications after acute myocardial infarction (AMI) are largely related to the presence of intraventricular conduction defects and not necessarily to symptoms.¹⁰ The requirement for temporary pacing with AMI does not inevitably constitute an indication for permanent pacing.²⁵ The long-term prognosis for survivors of AMI is related primarily to the extent of myocardial injury and nature of intraventricular conduction defects rather than to AVHB itself.^{10,34,45–48} With the exception of isolated left anterior fascicular block, AMI patients with intraventricular conduction disturbances have unfavorable short- and long-term prognoses, with increased risk of sudden death.^{10,34,45,47} This prognosis is not necessarily due to the development of high-grade AVHB,¹⁰ although the incidence of high-grade AVHB is higher among these patients.^{45,49} Pacing indications for AVHB after AMI are listed in table 4.¹⁰

Sinus Node Dysfunction. Sinus node dysfunction may manifest as sinus bradycardia, sinus pause or arrest,

or sinoatrial block, with or without escape rhythms. It often occurs in association with paroxysmal supraventricular tachydysrhythmias (bradycardia-tachycardia syndrome). Sinus bradycardia due to increased vagal tone is physiologic in trained athletes, who may have sleeping heart rates as low as 30 beats/min, with sinus pauses or type I 2° AVHB.¹⁰ Patients with sinus node dysfunction may have symptoms due to bradycardia, tachycardia, or both. Correlation of symptoms with dysrhythmias is essential¹⁰ and is established by ambulatory monitoring. Sinus node dysfunction may also present as a deficient rate response to stress or exercise (*i.e.*, chronotropic incompetence). An adaptive-rate pacemaker may benefit these patients by restoring more physiologic heart rates.^{10,50,51} Although sinus node dysfunction is often the primary indication for a pacemaker,⁵⁰ pacing does not necessarily improve survival.^{52,53} However, symptoms due to bradycardia may be relieved. Nonrandomized studies suggest that dual-chamber pacing improves survival more than ventricular pacing.¹⁰ A single randomized, prospective trial of atrial *versus* ventricular pacing found significantly higher rates of survival, less atrial fibrillation, fewer thromboembolic compli-

Table 3. Indications for Permanent Pacing with Long-term Bifascicular and Trifascicular Block

Class I—Indicated	Class II—May Be Indicated	Class III—Not Indicated
Intermittent 3° AVHB associated with symptoms Type II, 2° AVHB with symptoms	BFB or TFB block with syncope not proven due to AVHB, but other causes of syncope are not identifiable (specifically, VT) HV interval > 100 ms or pacing-induced infra-Hisian block	BFB or TFB without AVHB or symptoms BFB or TFB with 1° AVHB without symptoms

AVHB = atrioventricular heart block; BFB or TFB = bifascicular or trifascicular block; VT = ventricular tachycardia; HV interval = His-Purkinje conduction time. Adapted from Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *J Am Coll Cardiol* 1998; 31:1175–209. Copyright 1998 by the American College of Cardiology and the American Heart Association. Permission granted for one-time use. Further reproduction is not permitted without permission of the ACC/AHA.

Table 6. Indications for Pacing with Hypersensitive Carotid Sinus and Neurally Mediated Syndromes

Class I—Indicated	Class II—May Be Indicated	Class III—Not Indicated
Recurrent syncope caused by carotid sinus stimulation; minimal carotid sinus pressure induces asystole > 3 s duration in the absence of drugs that depress the sinus node or atrioventricular conduction	Recurrent syncope without clear provocative events and with a hypersensitive cardioinhibitory response Neurally mediated syncope with significant bradycardia reproduced by a head-up tilt with or without provocative maneuvers (isoproterenol)	Hyperactive cardioinhibitory response to carotid sinus stimulation, but no symptoms Hyperactive cardioinhibitory response to carotid sinus stimulation with vague symptoms such as dizziness, light-headedness, or both Recurrent syncope, light-headedness, or dizziness in the absence of a hyperactive cardioinhibitory response Situational vasovagal syncope in which avoidance behavior is effective

Adapted from Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *J Am Coll Cardiol* 1998; 31:1175–209. Copyright 1998 by the American College of Cardiology and the American Heart Association. Permission granted for one-time use. Further reproduction is not permitted without permission of the ACC/AHA.

of the natural history of the disease, as well as advances in technology and diagnosis. For example, pacing may improve long-term survival and prevent syncope in selected patients with congenital complete AVHB.^{58,59} A number of criteria, including average heart rate, QT interval duration, exercise tolerance, and associated structural heart disease, are weighed before pacemaker implantation in asymptomatic patients.¹⁰

For patients with chronic advanced 2° or 3° AVHB following cardiac surgery, the prognosis is poor without pacing.⁶⁰ However, the need for pacing in patients with residual bifascicular heart block and intermittent AVHB is less certain.¹⁰ Before a device is implanted, the embolic risk of residual intracardiac defects and requirement for lifelong pacing must be considered. The bradycardia-tachycardia syndrome commonly occurs following congenital heart surgery.⁶¹ Both antibradycardia and ATP have been used for treatment,^{62,63} but the results are equivocal.^{10,61,64,65} Nonetheless, symptomatic bradycardia and proarrhythmia with drugs (*i.e.*, provocation of new or worse dysrhythmias) limit their usefulness for treatment. Thus, pacing is weighed as adjunctive therapy for the bradycardia-tachycardia syndrome.¹⁰ Finally, the use of pacing and β -blockers in patients with congenital long QT syndrome has support,^{66,67} especially in cases of pause-dependent ventricular tachydysrhythmias. Pacing indications for children and adolescents are summarized in table 7.¹⁰

Miscellaneous Pacing Indications.

Hypertrophic Obstructive Cardiomyopathy. A dual-chamber pacemaker with a short atrioventricular delay reduces the magnitude of left-ventricular outflow tract obstruction and alleviates symptoms in patients with severely symptomatic obstructive hypertrophic cardiomyopathy.^{68–70} Recent trials confirm this and also demonstrate improvement in functional status.^{71,72} However, the perceived symptomatic improvement may be little more than a placebo effect.^{73,74} Mechanisms by

which pacing might improve the LV outflow obstruction are unclear but possibly involve changes in the ventricular contraction pattern.¹⁰ Selection of optimal atrioventricular delay appears critical to achieving a beneficial hemodynamic result.^{70,75}

Dilated Cardiomyopathy. Several observational studies show hemodynamic improvement after institution of dual-chamber pacing with short atrioventricular delay for dilated cardiomyopathy.^{76–79} Possibly, well-timed atrial contractions prime the ventricles and decrease mitral regurgitation, thereby augmenting stroke volume and arterial pressure.¹⁰ Greater improvement may be obtained with atrioventricular synchronous biventricular pacing than with single-site right ventricular pacing in patients with intraventricular conduction block and end-stage heart failure.⁸⁰

Cardiac Transplantation. The incidence of bradydysrhythmias after cardiac transplantation ranges from 8 to 23%, with the majority of occurrences due to sinus node dysfunction.¹⁰ Because of symptoms and delayed rehabilitation, some centers are more aggressive with pacing for persistent postoperative bradycardia. However, because one half of patients with bradydysrhythmias after cardiac transplantation show improvement by 1 yr, long-term pacing may be unnecessary.^{10,81,82}

Termination and Prevention of Tachydysrhythmias by Pacing. Pacing can terminate a variety of tachydysrhythmias, including atrial flutter, paroxysmal reentrant supraventricular tachycardia (SVT), and ventricular tachycardia (VT).¹⁰ A number of pacing patterns are used, including programmed extrastimulation and short bursts of rapid pacing. Although use of dedicated antitachycardia pacemakers has been reported,⁸³ today this capability is more likely to be incorporated in an ICD device as part of a tiered antidysrhythmia therapy (below). Pacing and β -blockers are used to prevent dysrhythmias with congenital long QT syndrome^{66,67} and to

Table 7. Indications for Pacing in Children and Adolescents

Class I—Indicated	Class II—May Be Indicated	Class III—Not Indicated
Advanced 2° or 3° AVHB with symptomatic bradycardia, low cardiac output, or CHF	BTS with the need for long-term antiarrhythmic drug treatment (except digitalis)	Transient postoperative AVHB: return of normal atrioventricular conduction within 7 days
SND with correlation of symptoms during age-inappropriate bradycardia	Congenital 3° AVHB after age 1 yr; average rate < 50 beats/min or pauses 2–3× basic cycle length	Postoperative bifascicular block, with or without 1° AVHB, and no symptoms
Postoperative 2° or 3° AVHB not expected to resolve or that persists at least 7 days	LQTS with type II, 2° or 3° AVHB	Asymptomatic type I, 2° AVHB
Congenital 3° AVHB with wide QRS escape rhythm or ventricular dysfunction	Complex CHD: asymptomatic sinus bradycardia with resting rate < 35 beats/min or pauses > 3 s	Sinus bradycardia without symptoms in adolescents with CHD, when longest R-R interval is < 3 s and minimum rate > 40 beats/min
Congenital 3° AVHB in an infant with rates < 50–55 beats/min or CHD and rates < 70 beats/min	Transient postoperative 3° AVHB; return of normal atrioventricular conduction by 7 days	
Sustained, pause-dependent VT, with or without long QT, in which the efficacy of pacing is thoroughly documented	Asymptomatic postoperative bifascicular block, with or without 1° AVHB	
	Asymptomatic type I, 2° AVHB	
	Adolescents: asymptomatic sinus bradycardia (longest R-R interval < 3 s; minimum rate > 40 beats/min)	

AVHB = atrioventricular heart block; CHF = congestive heart failure; SND = sinus node dysfunction; CHD = congenital heart disease; VT = ventricular tachycardia; BTS = bradycardia-tachycardia syndrome; LQTS = long QT syndrome.

Adapted from Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *J Am Coll Cardiol* 1998; 31:1175–209. Copyright 1998 by the American College of Cardiology and the American Heart Association. Permission granted for one-time use. Further reproduction is not permitted without permission of the ACC/AHA.

prevent recurrences of paroxysmal SVT⁸⁴ and bradycardia-dependent atrial fibrillation.^{85–88}

Indications for ICDs

An ICD can be used for the prevention of sudden death in a patient with life-threatening ventricular tachydysrhythmias.¹⁰ An implanted atrial ICD⁸⁹ or combined atrial and ventricular ICD⁹⁰ may be prescribed for patients with paroxysmal atrial tachydysrhythmias or susceptibility to both atrial and ventricular tachydysrhythmias. However, there is no consensus with regard to indications for use of these devices.

It has been clearly shown in prospective clinical trials that ICDs revert sustained VT and ventricular fibrillation (VF). ICDs terminate VF successfully in more than 98% of episodes.^{91,92} When an ICD is used with tiered therapy, VT is converted with ATP in 89%⁹¹ to 96%⁹³ of episodes. Inappropriate ICD therapy, namely, high-energy shocks delivered for misdiagnosed dysrhythmias, is administered to 5–11% of patients. Availability of stored events has made it possible to estimate the benefit of ICDs in the absence of placebo-controlled studies.^{94–97} In these studies, ICDs have achieved greater than 98% conversion of VF or VT with circulatory collapse, with a significant projected survival benefit in comparison with that in untreated populations.⁹⁴ This benefit is incremental and continues to increase up to 4 yr. A similar benefit exists for patients with sustained VT.⁹⁵ In addition, survival of patients with ICDs is influenced by left ventricular function. Survival among patients with a left ventricular ejection fraction greater than or equal to 30% is lower at 3 yr than among those with higher ejection fractions.^{98,99}

However, both groups derive a significant survival benefit with ICDs in comparison with the benefit of drug treatment alone.¹⁰⁰

Drugs and surgical or catheter ablation are other options to reduce or prevent VT or VF in at-risk patients, although drugs and ICDs together may improve quality of life by reducing the need for shocks.¹⁰ Whereas serial electrophysiologic testing or Holter monitoring is used to guide drug therapy, maintaining effective therapy may be difficult because of intolerance and prodysrhythmia or adverse effects with prolonged use.^{101,102} Although β -blockers do reduce mortality after acute infarction,^{103,104} there are no data to support the use of β -blockers as single therapy for ventricular tachydysrhythmias.^{10,100} Class III drugs, especially amiodarone, are associated with significantly lower rates of tachydysrhythmia recurrence, sudden death, and total mortality.^{10,100} AVID, a large, prospective, randomized trial, compared long-term therapy with ICDs and class III drugs for survivors of cardiac arrest and patients with unstable VT.¹⁰⁰ For ICDs and drugs, unadjusted survival estimates at 1 yr were 89% and 82%; at 2 yr, 82% and 75%; and at 3 yr, 75% and 64%, respectively. With ICDs, the estimated relative risk reduction was 39% at 1 yr and 31% at 3 yr.

Radio-frequency current ablation is most effective for sustained monomorphic VT induced during electrophysiologic study or cardiac surgery and mapped to specific ventricular sites.¹⁰ Surgical experience is more extensive and favorable for patients with coronary disease, and low recurrence rates (< 10% at 2 yr) and minimal sudden death rates have been reported.^{105–107}

Table 8. Indications for ICD Therapy for Primary or Secondary Prevention

Class I—Indicated	Class II—May Be Indicated	Class III—Not Indicated
Cardiac arrest due to VT/VF not due to a transient or reversible cause	Cardiac arrest presumed due to VT/VF: other medical conditions preclude EPS	Syncope of undetermined cause; no inducible VT/VF
Spontaneous sustained VT	Severely symptomatic VT before heart transplantation	Incessant VT/VF
Syncope of undetermined origin with clinically relevant, hemodynamically significant sustained VT or VF induced at EPS when drug therapy is ineffective, not tolerated, or not preferred	LQTS, HCM, and other familial conditions with a high risk for life-threatening ventricular dysrhythmias	VT/VF consequent to SVT or VT amenable to surgical or catheter ablation (WPW; specific types of VT*)
NSVT with CAD, previous MI, LV dysfunction, and inducible VF or sustained VT at EPS not suppressed by a class I antidysrhythmia	Inducible sustained VT/VF in patient with NSVT, CAD, old MI, and LV dysfunction	Ventricular VT/VF due to a transient or reversible cause
	Recurrent syncope of undetermined etiology in the presence of ventricular dysfunction and inducible ventricular dysrhythmias at EPS if other causes of syncope have been excluded	Psychiatric illnesses that may be aggravated by ICD implantation or precludes systematic follow-up
		Terminal illness with ≤ 6 months life expectancy
		After CABG: prolonged QRS; LV dysfunction; no spontaneous/inducible VT
		Drug-refractory, Class IV (NYHA) CHF: not candidate for heart transplantation

* Specific VT includes idiopathic left ventricular, right ventricular outflow tract, and bundle branch or fascicular VT.

VT = ventricular tachycardia; VF = ventricular fibrillation; EPS = electrophysiological study; NSVT = nonsustained VT; CAD = coronary artery disease; MI = myocardial infarction; LV = left ventricular; LQTS = long QT syndrome; HCM = hypertrophic cardiomyopathy; SVT = supraventricular tachydysrhythmias; WPW = Wolff-Parkinson-White syndrome; ICD = internal cardioverter-defibrillator; CABG = coronary artery bypass surgery; NYHA = New York Heart Association.

Adapted from Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *J Am Coll Cardiol* 1998; 31:1175-209. Copyright 1998 by the American College of Cardiology and the American Heart Association. Permission granted for one-time use. Further reproduction is not permitted without permission of the ACC/AHA.

Catheter ablation is most effective with right ventricular outflow tract VT, idiopathic left septal VT, and bundle branch reentrant VT.¹⁰⁸⁻¹¹⁰ Multiple VT morphologies and polymorphic VT, along with progressive cardiomyopathy, are less amenable to a favorable result with catheter ablation.¹⁰

Use of ICDs is prescribed for secondary prevention in patients who have coronary artery disease and a history of sudden death or who have documented or inducible sustained ventricular tachydysrhythmias.¹⁰ Such patients account for the majority of those receiving ICDs.¹⁰ ICDs are widely accepted for improving outcomes for these patients. ICDs are also indicated for patients with long QT syndrome and recurrent syncope, sustained ventricular dysrhythmias, or sudden cardiac death despite drug therapy.^{67,111,112} ICDs are prescribed along with class IA antidysrhythmic drugs (mostly quinidine) for patients with idiopathic VF or the Brugada syndrome.¹¹³ The latter is the association of right bundle-branch block and ST-segment elevation (electrocardiographic leads V1-V3) with sudden death in patients without confirmed heart disease.^{114,115} Sudden death survivors with hypertrophic cardiomyopathy are considered for ICD therapy in preference to or with drugs.^{10,116} ICDs are used as prophylaxis for syncope and sudden death with drug-refractory dysrhythmias and dysrhythmogenic right ventricular dysplasia.¹¹⁷ Fewer than 1% of ICD implants are for primary prevention in pediatric patients.¹¹⁸ However, the need for lifelong drug therapy, with possible noncompliance and adverse effects, makes ICDs an im-

portant treatment option for young patients with congenital heart disease, cardiomyopathies, or primary electrical disease (e.g., long QT syndrome), patients with malignant dysrhythmias, and sudden death survivors.¹⁰ A family history of sudden death may also influence the decision to implant an ICD.^{67,111,119}

Finally, ICDs are used for primary prevention in patients with asymptomatic coronary artery disease and nonsustained ventricular tachydysrhythmias.^{112,120} Other circumstances in which ICDs have been used for primary prevention include following coronary artery bypass surgery in patients with severe left ventricular dysfunction (ejection fraction < 35%) and after abnormal findings of signal-averaged electrocardiography,¹²¹ as well as in some patients awaiting heart transplantation.^{10, 122, 123} However, with the latter, the benefit is diluted by some patients' death due to heart failure. Indications for ICDs are summarized in table 8.¹⁰

Device Selection

Temporary Pacing. Transvenous (endocardial), epicardial, transesophageal, and transcutaneous routes are used for temporary pacing. The first two routes are considered invasive (e.g., risk of sepsis, direct myocardial damage, or cardiac perforation with tamponade), and the latter two pacing routes are considered noninvasive. Discussion of the pros and cons of each, as well as methods and equipment, is beyond the scope of this article. The interested reader is referred to previous publications.^{16,18,19,24}

Selection of a Permanent Pacemaker. Single- and dual-chamber pulse generators vary in size, battery capacity, cost, and unipolar or bipolar electrode configuration (below). They may incorporate sensor-modulated adaptive-rate pacing, programmable polarity, and/or automatic mode-switching. Pacing leads vary in electrode configuration, insulation material, methods for fixation, stimulation impedance, and presence of steroid elution. Other factors that influence pacemaker selection are the pacemaker programming device capabilities and access to technical support. For all devices, pacing mode, pulse amplitude and width, sensitivity, lower rate, and refractory periods are programmable. For dual-chamber devices, the atrioventricular interval and maximum tracking rate are also programmable. With adaptive-rate pacemakers, several rate-modulation parameters are programmable. Implanting physicians must also anticipate the progression of cardiac rhythm abnormalities when selecting and programming a device.¹⁰ For example, patients with sinus node dysfunction and susceptibility to paroxysmal atrial tachyarrhythmias might develop AVHB due to needed drug therapy, disease progression, or catheter ablation for modification of atrioventricular conduction. If so, a dual-chamber pacemaker with automatic mode-switching might be indicated. Finally, the patient with an indication for pacing and at risk for VT or VF will receive a single- or dual-chamber ICD, since all ICDs today have a single- or dual-chamber pacing capability, and many have adaptive-rate pacing as well.

Adaptive-rate Pacemakers. A 1996 industry-wide survey in the United States indicated that adaptive-rate pacing was a programmable option in 83% of all implanted pulse generators.¹⁰ In patients with chronotropic incompetence, adaptive-rate pacing improves exercise capacity and quality of life.¹⁰ Most sensors are piezoelectric crystals or accelerometers that detect motion, acceleration, vibration, or pressure.^{10,124} Nevertheless, minute ventilation¹²⁵ or stimulus-to-T interval¹²⁶ sensors may provide a rate response more proportional to exercise.¹⁰

Single-pass Lead Systems. Commonly, dual-chamber devices have a separate atrial lead to detect atrial depolarization in patients with sinus node dysfunction. Single-pass leads have both atrial and ventricular electrodes, negating the need for separate leads.⁶ However, it was found that the amplitude of sensed signals with separate, floating atrial leads was inconsistent and varied significantly with changes in posture.^{127,128} In addition, atrial pacing was not possible. With newer, single-pass leads, the atrial signal amplitude is higher and dual-chamber pacing is possible.^{129,130}

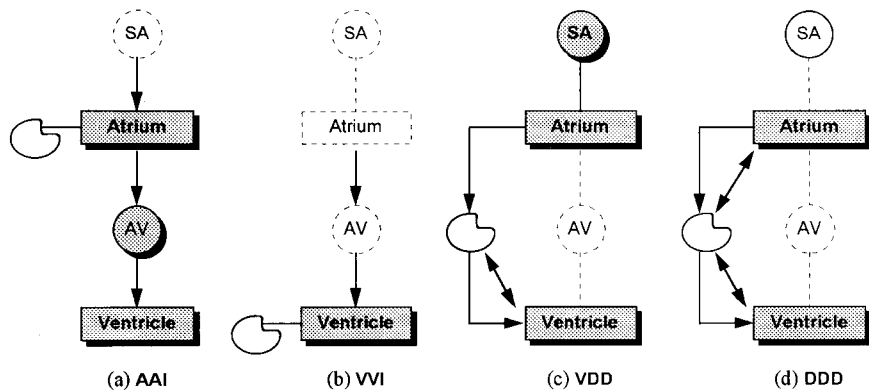
Programmable Lead Configuration and Automatic Mode-switching. Most contemporary pacemakers offer separately programmable lead configurations for both pacing and sensing in the atrium and ventricle.⁶ Thus, if the pacing system uses bipolar leads, it is possi-

ble to noninvasively switch back and forth between unipolar and bipolar lead configurations. With the former, all or part all of the pulse generator metal housing (can) serves as the anode (+) and the distal electrode of the bipolar lead as cathode (-). With the bipolar configuration, proximal and distal lead electrodes serve as anode and cathode, respectively. The ability to program unipolar pacing is necessary if lead insulation or conductor failure occurs in a bipolar lead system.⁶ In addition, the ability to program separate lead configurations for sensing and pacing permits exploitation of either while minimizing disadvantages (e.g., oversensing with unipolar leads).^{5,6} Dual-chamber pacemakers with automatic mode-switching are used for patients with AVHB and susceptibility to paroxysmal atrial tachyarrhythmias. Algorithms detect rapid, nonphysiologic atrial rates and automatically switch the pacing mode to one that excludes atrial tracking and the associated risk of ventricular pacing at or near the programmed maximal rate.^{7-9,131}

Pacemaker Leads. Most contemporary pacemakers use transvenous (endocardial) leads. Bipolar leads are being used increasingly worldwide.⁶ Bipolar sensing reduces risk of inappropriate pacing inhibition or stimulation due to oversensing. However, with some bipolar leads, there has been an unacceptably high failure rate due to lead insulation degradation,¹⁰ although newer lead designs have improved on this.^{132,133} An important advance has been development of steroid-eluting leads.^{6,10} These have a small reservoir of corticosteroid that is slowly released into the electrode-tissue interface, reducing inflammation, fibrosis, and chronic capture thresholds.

Selection of an ICD. Many of the above considerations apply to ICD selection, since they feature antibradycardia pacing as well as ATP and shocks for tachyarrhythmias. A primary feature that distinguishes contemporary ICDs from earlier models is the availability of ATP as a programmable option. Although ATP increases pulse generator cost, it is useful in a majority of patients receiving ICDs, since it converts up to 96% of episodes of VT without the need for shocks.⁹³ Nonetheless, ATP may accelerate VT in 2-6% of episodes,^{93,134,135} although this may be influenced by whether the pacing algorithm to terminate VT is used empirically or on the basis of results of electrophysiologic testing.¹³⁵ Patients with only VF before ICD implantation are less likely to subsequently have VT detected by their ICDs.¹³⁶ However, the incidence of VT in these patients (18%) is significant¹³⁶; thus, it is desirable to have ATP as a programmable feature of ICDs, even without a history of VT.^{4,10} Finally, ICDs with dual-chamber pacing and sensing are appropriate for patients who require dual-chamber pacing and therapy for VT or VF or who have atrial dysrhythmias that might trigger inappropriate ICD therapies.¹⁰

Fig. 1. Examples of antibradycardia pacing modes. (A) Atrial-inhibited (AAI) pacing for sinus arrest or bradycardia. The pulse generator is shown with atrial leads only. The atrium is paced, unless pacing is inhibited by sensed spontaneous atrial depolarizations. (B) Ventricular-inhibited (VVI) pacing for atrioventricular (AV) heart block (AVHB) with atrial fibrillation. The pulse generator is shown with ventricular leads only. The ventricle is paced, unless pacing is inhibited by sensed spontaneous ventricular depolarizations. (C) Ventricular-inhibited, atrial-triggered (VDD) pacing for AVHB with normal sinoatrial (SA) node and atrial function. The pulse generator is attached to atrial leads for sensing only and to ventricular leads for pacing and sensing. If a spontaneous atrial depolarization is sensed, the ventricle is paced after an appropriate atrioventricular interval to permit ventricular filling. This is the atrial-triggered ventricular pacing (VAT) component of the VDD mode, which also includes capabilities of the VVI mode. (D) Dual-chamber sequential or atrioventricular universal (DDD) pacing for sinus bradycardia and AVHB. The pulse generator is shown attached to atrial and ventricular leads for dual-chamber sensing and pacing. This mode incorporates AAI, VVI, and VAT pacing capabilities. Reprinted with permission from Bernstein AD, Parsonnet V: Fundamentals of antibradycardia-pacemaker timing. ACC Educational Highlights 1995; 11:5-9; copyright American College of Cardiology.



Device Design and Function

Pacemaker Design and Function. Pacemakers are powered by lithium-iodide batteries, with an expected service life of 5-12 yr, depending on device capabilities. Actual service life will depend on the need for pacing and the programmed stimulus parameters. Most systems use bipolar transvenous leads. These are positioned under fluoroscopic guidance, with the lead configuration programmable (above). A single-chamber pacemaker stimulates the atria or ventricles on the basis of programmed timing intervals. In addition, by sensing intrinsic atrial and/or ventricular depolarizations, it can be inhibited from providing unnecessary or inappropriate stimuli. Dual-chamber devices also time delivery of ventricular stimuli relative to sensed atrial depolarizations to maintain proper atrioventricular synchrony. In figure 1, we illustrate how a pacemaker might be configured to pace in patients with sinus node dysfunction or AVHB. Throughout the remainder of the current article and in the sequel, the North American Society for Pacing and

Electrophysiology-British Pacing and Electrophysiology Group (NASPE/BPEG) pacemaker code (sometimes called NBG code; table 9) is used as shorthand to describe pacing modes.¹³⁷

Timing Design: Single-chamber Pacemakers. Today, most pacemakers in the United States are conventional or adaptive-rate, dual-chamber devices.¹⁰ However, with normal atrioventricular conduction and sinus node function, they may operate as single-chamber devices, in the AAI/AAIR or VVI/VVIR modes, depicted in figure 1. They have a single timing interval, the interval between stimuli in the absence of sensed depolarization. For single-chamber pacing modes, this interval is the atrial or ventricular escape interval. It is inversely proportional to the pacing rate in paced pulses per minute (ppm):

$$\text{Escape interval (ms)} = 60,000/\text{rate (ppm)}$$

In the AAI mode (fig. 2), pacing will occur at the end of the programmed atrial escape interval, unless a spon-

Table 9. The NASPE-BPEG Generic (NBG) Pacemaker Code

I	II	III	IV	V
Chamber Paced	Chamber Sensed	Response to Sensed Event	Programmability/Rate Response*	Antitachycardia Functions†
O (none)	O (none)	O (none)	O (none)	O (none)
A (atrium)	A (atrium)	I (inhibit)	R (adaptive rate)	P (ATP)
V (ventricle)	V (ventricle)	T (triggered)	P (simple programmable)	S (shock)
D (dual: A + V)	D (dual: A + V)	D (I and T)	M (multiprogrammable)	D (dual: P + S)
S (single)‡	S (single)‡		C (communicating)	

* In current terminology, only the adaptive rate response (R) is indicated by the fourth position; all current pacemakers have full programming and communicating capability. Therefore, the letters P, M, and C are no longer used.

† ICD with antibradycardia and antitachycardia pacing capabilities.

‡ Single-chamber device that paces either the atrium or ventricle.

ATP = antitachycardia pacing.

From Bernstein AD, Camm AJ, Fletcher RD, Gold RD, Rickards AF, Smyth NP, Spielman SR, Sutton R: The NASPE/BPEG generic pacemaker code for antibradyarrhythmia and adaptive-rate pacing and antitachyarrhythmia devices. Pacing Clin Electrophysiol 1987; 10:794-9. Used with permission.

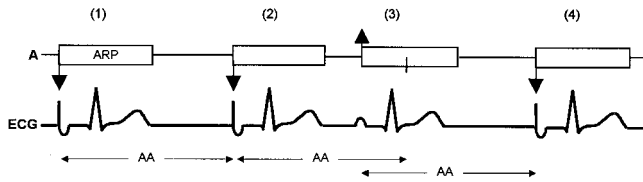


Fig. 2. Depiction of atrial-inhibited pacing, as for sinus bradycardia with intact atrioventricular conduction. In the first beat, the atrium (A) is paced (by convention, an arrow pointing toward the electrocardiogram [ECG] in the atrial timing diagram). The atrial refractory period (ARP) prevents conducted R and ensuing T waves from being interpreted by the device as a P wave and inappropriately resetting the atrial escape interval (AA). After the programmed AA interval, another atrial stimulus occurs and resets the interval. In the third beat, a spontaneous P wave is sensed (by convention, an arrow pointing away from the electrocardiogram in the atrial timing diagram) before the AA interval times out. This resets the AA interval without pacing (the short vertical line in the atrial timing diagram shows where the stimulus would have occurred). In the absence of further sensing, the atrium is paced in the fourth beat when the AA interval times out. This example illustrates a principle that is useful for interpreting a single-chamber pacemaker electrocardiogram. Once the escape interval is known (from the clinical records, device telemetry, or measurement between consecutive paced beats), electrocardiographic interpretation is facilitated by working backward from the last stimulus to identify the sensed event that reset the pacemaker's escape timing as a P wave (or R wave, as the case may be), and not a spurious signal. Reprinted with permission from Bernstein AD, Parsonnet V: Fundamentals of antibradycardia-pacemaker timing. ACC Educational Highlights 1995; 11:5-9; copyright American College of Cardiology.

taneous atrial depolarization is sensed first and resets the interval. Stimulus timing is identical for the VVI mode (fig. 3). Ventricular pacing will occur at the end of the ventricular escape interval, unless a spontaneous ventricular depolarization is sensed first and resets the interval. Because of this timing similarity, some single-chamber pacemakers can be used with pacing leads in either the

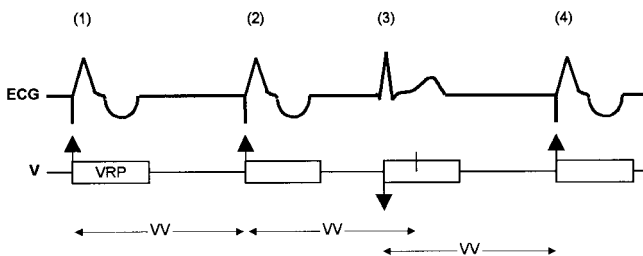


Fig. 3. Depiction of ventricular-inhibited pacing, as for atrioventricular heart block with atrial fibrillation. In the first beat, the ventricle (V) is paced. The pacemaker's ventricular refractory period (VRP) prevents the ensuing T wave from being interpreted as an R wave and inappropriately resetting the ventricular escape interval (VV). The programmed VV interval times out with delivery of a ventricular stimulus and resets the VV interval. However, a spontaneous R wave (third beat) is sensed before this times out. It inhibits the ventricular stimulus that would have occurred (short vertical line in the ventricular-channel timing diagram) and resets the VV interval. With no further sensing, pacing occurs when the VV interval times out (fourth beat). ECG = electrocardiogram. Reprinted with permission from Bernstein AD, Parsonnet V: Fundamentals of antibradycardia-pacemaker timing. ACC Educational Highlights 1995; 11:5-9; copyright American College of Cardiology.

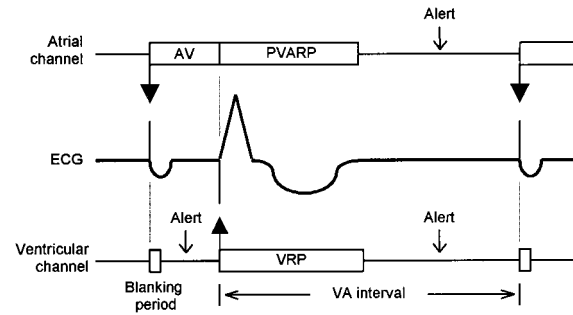


Fig. 4. Basic timing of a dual-chamber pacemaker, with pacing and sensing in both chambers. Atrial and ventricular stimuli are shown in the timing diagrams by arrows pointing toward the electrocardiogram (ECG) from above and below, respectively. The programmed atrioventricular (AV) interval provides time for ventricular filling. The atrial channel is refractory during the atrioventricular interval and from delivery of the ventricular stimulus until the end of the programmed postventricular atrial refractory period (PVARP). This prevents atrial sensing from resetting the escape timing. The blanking period (ventricular channel) prevents sensing of the atrial stimulus. However, sensing in the alert period after the blanking period would enable a spontaneous R wave to reset the interval between the ventricular stimulus or sensed spontaneous R wave and the subsequent atrial stimulus (the VA interval), thereby inhibiting ventricular stimulation. As shown, this does not occur, so the atrioventricular interval times out with delivery of a ventricular stimulus. The ventricular refractory period (VRP) prevents sensed T waves from inappropriately resetting the VA interval. Sensing during the alert periods after the PVARP and VRP will reset basic timing, initiating new atrioventricular and VA intervals, respectively. Reprinted with permission from Bernstein AD, Parsonnet V: Fundamentals of antibradycardia-pacemaker timing. ACC Educational Highlights 1995; 11:5-9; copyright American College of Cardiology.

atrium or the ventricle. In addition, some single-chamber pacemakers offer rate hysteresis as a programmable option. With this, the atrial or ventricular escape interval after a sensed depolarization is longer than that after a paced depolarization. Rate hysteresis encourages the emergence of an intrinsic rhythm, thereby reducing the likelihood of competition between paced and spontaneous rhythm and prolonging battery life.

Timing Design: Dual-chamber Pacemakers. Figure 4 illustrates the basic timing design of a dual-chamber pacemaker that can pace and sense in both the atrium and the ventricle. Dual-chamber pacemakers have two basic timing intervals, whose sum is the pacing-cycle duration. The first is the atrioventricular interval, which is the programmed interval from a paced or sensed atrial depolarization to the subsequent ventricular stimulus. Some dual-chamber pacemakers offer the option of programmable atrioventricular interval hysteresis. If so, the atrioventricular interval after an atrial stimulus is longer than that following a sensed spontaneous P wave to maintain a uniform interval between atrial and ventricular contractions. The second basic timing interval is the VA interval, the interval between a ventricular stimulus or sensed spontaneous R wave and the subsequent atrial stimulus. During the pacemaker's atrial and ventricular refractory periods (fig. 4), sensed

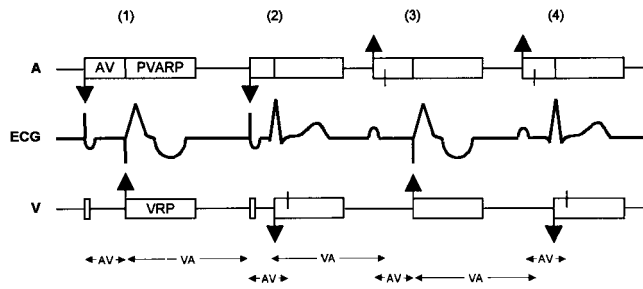


Fig. 5. Basic patterns in dual-chamber pacing. The first beat is fully paced and is an example of atrioventricular (AV) sequential pacing. In the second beat, a spontaneous R wave is sensed in the ventricular (V) channel before the atrioventricular interval times out, initiating a new VA interval (the interval between the ventricular stimulus or sensed spontaneous R wave and the subsequent atrial stimulus). Thus, it inhibits the ventricular stimulus that would have occurred (short vertical line in the ventricular-channel timing diagram). In the third beat, a P wave is sensed in the atrial (A) channel before the VA interval times out, initiating a new atrioventricular interval. It also inhibits the stimulus that would have occurred (short vertical line in the atrial-channel timing diagram). This is an example of atrial synchronous ventricular pacing, which is equivalent to the VAT mode (fig. 1). In the last beat, spontaneous P and R waves are sensed before the respective VA and atrioventricular intervals time out. ECG = electrocardiogram; PVARP = postventricular atrial refractory period; VRP = ventricular refractory period. Reprinted with permission from Bernstein AD, Parsonnet V: Fundamentals of antibradycardia-pacemaker timing. ACC Educational Highlights 1995; 11:5-9; copyright American College of Cardiology.

events do not reset the device's escape timing. During the ventricular channel blanking period (fig. 4), ventricular sensing is disabled to avoid overloading of the ventricular sense amplifier by voltage generated by the atrial stimulus. It also prevents the atrial stimulus from inappropriately resetting the VA interval without delivery of a ventricular stimulus. Sensing during alert periods after the post-ventricular atrial and ventricular refractory periods (fig. 4) resets basic pacemaker timing and initiates new atrioventricular or VA intervals, respectively.

A dual-chamber pacemaker provides atrioventricular sequential, atrial, ventricular, or no pacing, depending on the sensing patterns (fig. 5). Whenever sensing occurs outside the atrial or ventricular refractory periods or the blanking period, the current atrioventricular or VA interval is terminated without stimulation (fig. 5). The next timing interval begins at once. In addition, sensed R and P waves reset the atrial and ventricular timing intervals, respectively, without stimulus delivery (fig. 5).

Internal Cardioverter-Defibrillator Design and Function. An ICD system consists of a pulse generator and leads for tachydysrhythmia detection and therapy. ICDs provide antitachycardia and antibradycardia pacing, synchronized (cardioversion) or nonsynchronized (defibrillation) shocks, telemetry, and diagnostics, including stored event electrograms and history logs.^{4,138} Essentially, the pulse generator is a self-powered computer within a hermetically sealed titanium casing (can). One or two (in series) 3.2-V lithium-silver vanadium

oxide (SVO) batteries with high power density are used to power the pulse generator, circuitry, and aluminum electrolytic storage capacitors.¹³⁸ Most ICD designs use two capacitors in series to achieve a maximum voltage for defibrillation.¹³⁸ A major challenge in ICD design is the large range of voltages that must be controlled in a very small package. While monitored intracardiac signals may be as small as 100 μV , therapeutic defibrillatory shocks approach 750 V, with a leading edge of 15 amperes (A) and a pulse termination spike of 210 A.¹³⁸ Furthermore, because ICD batteries contain up to 20,000 joules (J), a potential hazard exists if the charging and firing circuits were to unload all this energy either electrically or thermally into the patient in a brief period.¹³⁸ Indeed, an ICD might reach a temperature of 85°C during a high-current state (e.g., a battery short or component failure within the high-voltage circuit).¹³⁸ Therefore, manufacturers reduce this hazard by use of current and thermal fuses in the power supplies.¹³⁸ In addition, the number of shocks delivered during treatment is usually limited to five or six per dysrhythmia.

Modern ICDs use transvenous lead systems for sensing, pacing, and shocks. Epicardial leads are still used in infants and small children. The expected service life is 5-8 years.^{53,138} Aside from the leads and battery, major subsystems of dual-chamber, adaptive-rate ICD pulse generators include (1) up to 100 kilobytes of ROM for system start-up tasks and some program space; (2) up to 512 kilobytes of RAM for additional program space and storage of operating parameters and lead electrogram data; (3) low-voltage supplies (3-15 V) for pacing and digital circuits and to control charging circuits; and (4) a high-voltage supply and output switching to generate and control delivery of high-energy, biphasic shocks.¹³⁸

Sensing of Ventricular Depolarizations by ICDs. Reliable sensing of ventricular depolarization is essential.^{4,138,139} The sense amplifier must respond quickly and accurately to rates of 30-360 beats/min or greater and to the varying amplitude and morphology of intracardiac signals during VT or VF. Unfiltered intracardiac electrograms are sent to the sense amplifier. This has a band-pass filter to reject low-frequency T waves and high-frequency noise, automatic gain control (autogain), a rectifier to eliminate polarity dependency, and a fixed or autoadjusting threshold event detector. The sense amplifier produces a set of R-R intervals for the VT and VF detection algorithms to use.

Because the amplitude of intracardiac ventricular electrograms can vary widely between sinus rhythm, VT, and VF, some form of autogain is required.^{4,138,139} If gain and sensitivity were fixed, as in pacemakers, and depending on the settings chosen, this could result in VT and VF undersensing or oversensing. In newer ICDs, digital, dynamic autogain continuously adjusts the gain so that the amplitude of the processed signal remains constant. An autoadjusting sensitivity threshold sets the sensitivity

to a proportion of the amplitude of the latest sensed event, and sensitivity then gradually increases until the next event is sensed. Sensed events are analyzed with use of a detection algorithm. This divides all possible ventricular rates into nonoverlapping rate zones (bradycardia, normal rate, VF, and up to three programmable VT zones).

VF Detection and Therapy by ICDs. The ICDs use rate criteria as the sole method for detecting VF.^{4,138,139} VF detection algorithms must have high sensitivity but low specificity. This is because the result of not detecting VF is grave. However, if criteria for tracking input signals are too aggressive, the ICD will likely oversense T waves during sinus rhythm. If too conservative, the device will likely undersense some VF but work very well during normal sinus rhythm. Even with autogain and autoadjusting sensitivity threshold, VF detection algorithms must tolerate some degree of undersensing. As a result, an ICD X/Y detector triggers when X of the previous Y sensed ventricular intervals (typically, 70–80% of intervals in a sliding window of 10–24 intervals) are shorter than the VF detection interval.¹³⁹ This mechanism successfully ignores the effect of a small number of undersensed events because of the small amplitude of VF intracardiac signals. Any tachycardia with a cycle length less than the VF detection interval will initiate VF therapy. After capacitor charging but before shock delivery, an algorithm confirms the presence of VF. After shock delivery, redetection and episode-termination algorithms determine whether VF has terminated, continued, or changed.

Successful defibrillation may require voltages 125 times greater than the battery voltage.^{4,138} This charge is stored in capacitors and delivered between high-energy electrodes to depolarize the ventricles, parts of which may be partially refractory and up to 10 cm away. Output switching is used during capacitor discharge to produce a biphasic shock waveform. In comparison with monophasic shocks, biphasic shocks greatly reduced defibrillation energy requirements^{140–142} and were critical to development of smaller ICDs suitable for pectoral implantation.

VT Detection and Therapy by ICDs. In contrast with VF detection algorithms, most VT algorithms in single-chamber ICDs require a programmable number of consecutive R-R intervals shorter than the VT detection interval.^{4,139} A longer R-R interval, as might occur during atrial fibrillation, would reset the VT counters. In patients with both supraventricular and ventricular tachydysrhythmias, up to 45% of ICD discharges may be inappropriate if rate is used as the sole criterion for VT therapy.¹⁴³ These are poorly tolerated by patients. To increase specificity, VT detection algorithm enhancements are programmed for one or more VT zones in single-chamber ICDs, including criteria for stability of rate, suddenness of onset, and intracardiac QRS mor-

phology.^{4,139} Enhancement criteria are not available in the VF zone, where maximum sensitivity is required. In addition, they are programmed only in rate zones that correspond to VT hemodynamically tolerated by the patient.

The rate stability criterion is used to distinguish sustained monomorphic VT with little cycle-length variation from atrial fibrillation with much greater cycle-length variation. For example, one algorithm operates when the VT count reaches four.¹³⁹ It then compares the latest R-R interval with each of the three preceding intervals. If the absolute value in milliseconds of any of the interval differences is greater than the programmed VT interval, the VT counter is reset to zero. Another algorithm calculates the R-R interval differences throughout a specified duration of tachycardia and then computes average variance on a beat-to-beat basis.¹³⁹ If R-R cycle-length variance at the end of the specified duration is greater than programmed for the VT zone, the rhythm is declared unstable (*i.e.*, not likely to be VT), and VT therapy is inhibited. The suddenness of onset criterion is used to distinguish sinus tachycardia from VT, since VT has a more sudden rate increase. For example, one algorithm finds the maximum difference between adjacent intervals for five intervals on each side of the lowest VT rate boundary.¹³⁹ When the maximum difference exceeds the programmable onset parameter by 9–34%, the algorithm selects the shorter of the two intervals as the pivot interval. Then, the difference between the average of four intervals before and three of four intervals after the pivot interval must also be greater than 9–34% to satisfy the onset criterion. Finally, morphology algorithms discriminate VT from SVT on the basis of morphology of intracardiac electrograms.¹³⁹ Morphology algorithms were not available in early ICDs because the required calculations were beyond the capabilities of then-available microprocessors. Discussion of the specific methods used for QRS waveform morphology analysis is beyond the scope of this article.¹³⁹

Insufficient specificity of VT detection algorithms, despite optimal enhancements, has been a significant problem with single-chamber ICDs. Dual-chamber ICDs have an atrial lead, which is used for bradycardia pacing and sensing for tachycardia discrimination.¹⁴⁴ Detection algorithms in dual-chamber ICDs use atrial and ventricular timing data to discriminate SVT from VT.¹³⁹ For example, the detection algorithm in the Gem DR and Jewel AF ICDs (Medtronic, Minneapolis, MN) is based on several fundamental design principles.¹³⁹ High sensitivity of single-chamber, rate-only detection is retained in the enhanced detection algorithm. The devices withhold VT/VF detection only if they can positively identify a specific SVT. The detection algorithm has four key elements: (1) the pattern of atrial and ventricular events; (2) atrial and ventricular rates; (3) regularity of R-R intervals; and (4) presence or absence of atrioventricular dissoci-

ation. The algorithm also uses two methods of atrial and ventricular pattern analysis, which are described and illustrated elsewhere.¹³⁹ Nonetheless, limitations of dual-chamber enhancement algorithms include (1) atrial far-field sensing of R waves, leading to rhythm misclassification, (2) trade-offs between undersensing and the necessity for dual-chamber blanking periods to prevent cross-sensing, and (3) distinguishing VT with 1:1 VA conduction from SVT with 1:1 atrioventricular conduction.¹³⁹

Treatment options for tachycardia in the VT zones include ATP, cardioversion, or defibrillation.^{4,139} Treatment progresses through a programmable sequence of responses (tiered therapy) until the episode is terminated. Most sustained monomorphic VT can be terminated by a critical pacing sequence.¹⁴⁵ With ATP, usually a train of stimuli are delivered at a fixed percentage of the VT cycle length. Repeated and more aggressive trains can be administered, resulting in termination of VT or progression to cardioversion or defibrillation. Pacing at faster rates increases the likelihood of VT termination and risk of acceleration. ATP is effective, with greater than 90% successful termination of spontaneous VT.^{146,147} ATP with backup defibrillation is well-tolerated and reduces the need for painful, high-energy shocks.¹⁴⁸ Finally, the efficacy of ATP and low-energy cardioversion is similar.¹⁴⁹ Both reduce the time to therapy and conserve ICD battery life.⁴

Bradycardia Pacing by ICDs. Ventricular demand pacing for bradycardia is a standard feature of all single-chamber ICDs. Dual-chamber ICDs have all the capabilities of dual-chamber pacemakers, including adaptive-rate pacing and automatic mode-switching. Approximately 20% of ICD recipients require bradycardia pacing, and 80% of these would benefit from dual-chamber pacing.¹⁵⁰ If one includes patients with severe ventricular dysfunction (ejection fraction < 20%) and who would benefit from dual-chamber sensing, it is possible that up to 50% of ICD recipients may benefit from the implantation of a dual-chamber ICD.^{4,151-152} Finally, pacing thresholds during pacing for VT and after defibrillation shocks are frequently higher than those needed for routine bradycardia pacing. Pacing thresholds for these conditions are separately programmable in dual-chamber ICDs.⁴

References

1. Furman S, Robinson G: The use of an intracardiac pacemaker in the correction of total heart block. *Surg Forum* 1958; 9:245-8
2. Mirowski M, Reid PR, Mower MM, Watkins L, Gott VL, Schauble JF, Langer A, Heilman MS, Kolenik SA, Fischell RE, Weisfeldt ML: Termination of malignant ventricular arrhythmias with an implanted automatic defibrillator in human beings. *N Engl J Med* 1980; 303:322-4
3. Barold S, Zipes D: Cardiac pacemakers and antiarrhythmic devices, *Heart Disease*, 5th edition. Edited by Braunwald E. Philadelphia, WB Saunders, 1997, pp 705-41
4. O'Callaghan PA, Rushkin JN: The implantable cardioverter defibrillator, *Hurst's The Heart*, 10th edition. Edited by Fuster V, Alexander RW, O'Rourke RA. New York, McGraw-Hill, 2001, pp 945-62
5. Exner DV, Rothschild JM, Heal S, Gillis AM: Unipolar sensing in contempo-

rary pacemakers: Using myopotential testing to define optimal sensitivity settings. *J Interv Cardiac Electrophysiol* 1998; 2:33-40

6. Mond HG: Engineering and clinical aspects of pacing leads, *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 127-50
7. Lam CT, Lau CP, Leung SK, Tse HF, Ayers G: Improved efficacy of mode switching during atrial fibrillation using automatic atrial sensitivity adjustment. *PACE* 1999; 22:17-25
8. Palma EC, Kedarnath V, Vankawalla V, Andrews CA, Hanson S, Furman S, Gross JN: Effect of varying atrial sensitivity, AV interval, and detection algorithm on automatic mode switching. *PACE* 1996; 19:1735-9
9. Ricci R, Puglisi A, Azzolini P, Spampinato A, Pignalberi C, Bellocci F, Adinolfi E, Dini P, Cavaglia S, De Seta F: Reliability of a new algorithm for automatic mode switching from DDDR to DDIR pacing mode in sinus node disease patients with chronotropic incompetence and recurrent paroxysmal atrial fibrillation. *PACE* 1996; 19:1719-23
10. Gregoratos G, Cheitlin M, Conill A, Epstein A, Fellows C, Ferguson TJ, Freedman R, Hlatky M, Naccarelli G, Saksena S, Schlant R, Silka M: ACC/AHA guidelines for implantation of cardiac pacemakers and antiarrhythmia devices: A report of the ACC/AHA Task Force on Practice Guidelines (Committee on Pacemaker Implantation). *Circulation* 1998; 97:1325-35
11. Schwartz M, Maglio C, Akhtar M, Sra J: Implantable atrial defibrillator and detection of atrial flutter. *J Interv Cardiac Electrophysiol* 2000; 4:257-9
12. Timmermans C, Levy S, Ayers GM, Jung W, Jordaens L, Rosenqvist M, Thibault B, Camm J, Rodriguez LM, Wellens HJ: Spontaneous episodes of atrial fibrillation after implantation of the Metrix Atrioverter: Observations on treated and nontreated episodes. *Metrix Investigators. J Am Coll Cardiol* 2000; 35:1428-33
13. Tse HF, Lau CP, Yomtov BM, Ayers GM: Implantable atrial defibrillator with a single-pass dual-electrode lead. *J Am Coll Cardiol* 1999; 33:1974-80
14. Tse HF, Lau CP, Sra JS, Crijns HJ, Edvardsson N, Kacet S, Wyse DG: Atrial fibrillation detection and R-wave synchronization by Metrix implantable atrial defibrillator: Implications for long-term efficacy and safety. *The Metrix Investigators. Circulation* 1999; 99:1446-51
15. Wellens HJ, Lau CP, Luderitz B, Akhtar M, Waldo AL, Camm AJ, Timmermans C, Tse HF, Jung W, Jordaens L, Ayers G: Atrioverter: An implantable device for the treatment of atrial fibrillation. *Circulation* 1998; 98:1651-6
16. Hayes DL, Holmes DR: Temporary cardiac pacing, *A Practice of Cardiac Pacing*. Edited by Furman S, Hayes DL, Holmes DR. Mt. Kisco, New York, Futura Publishing, 1993, pp 231-60
17. Francis GS, Williams SV, Achord JL, Reynolds WA, Fisch C, Friesinger GC 2nd, Klocke FJ, Akhtar M, Ryan TJ, Schlant RC: Clinical competence in insertion of a temporary transvenous ventricular pacemaker: A statement for physicians from the ACP/ACC/AHA Task Force on Clinical Privileges in Cardiology. *Circulation* 1994; 89:1913-6
18. Waldo AL, Henthorn RW, Epstein AE, Plumb VJ: Diagnosis and treatment of arrhythmias during and following open heart surgery. *Med Clin North Am* 1984; 68:1153-69
19. Bartecchi CE, Mann DE: Temporary Cardiac Pacing. Chicago, Precept Press, 1990, 321 pp
20. Benson DW Jr: Transesophageal electrocardiography and cardiac pacing: state of the art. *Circulation* 1987; 75(suppl III):86-92
21. Zoll PM: Noninvasive cardiac stimulation revisited. *PACE* 1990; 13:2014-6
22. Mitrani RD, Myerberg RJ, Castellanos A: Cardiac pacemakers, *Hurst's The Heart*. Edited by Fuster V, Alexander RW, O'Rourke RA. New York, McGraw-Hill, 2001, pp 963-92
23. Ryan TJ, Anderson JL, Antman EM, Braniff BA, Brooks NH, Califf RM, Hillis LD, Hiratzka LF, Rapaport E, Riegel BJ, Russell RO, Smith EE Jr, Weaver WD: ACC/AHA guidelines for the management of patients with acute myocardial infarction: A report of the American College of Cardiology/American Heart Association Task Force on Practice Guidelines (Committee on Management of Acute Myocardial Infarction). *J Am Coll Cardiol* 1996; 28:1328-428
24. Atlee JL: Cardiac pacing and electroversion, *Cardiac Anesthesia*, 4th edition. Edited by Kaplan JA. Philadelphia, WB Saunders, 1999, pp 959-89
25. Ellenbogen KA, Guzman MA, Kawanishi DT, Rahimtoola SH: Pacing for acute and chronic atrioventricular conduction system disease, *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 426-53
26. Mymin D, Mathewson FA, Tate RB, Manfreda J: The natural history of primary first-degree atrioventricular heart block. *N Engl J Med* 1986; 315:1183-7
27. Barold SS: Indications for permanent cardiac pacing in first-degree AV block: class I, II, or III? (editorial). *PACE* 1996; 19:747-51
28. Kim YH, O'Nunain S, Trouton T, Sosa-Suarez G, Levine RA, Garan H, Ruskin JN: Pseudo-pacemaker syndrome following inadvertent fast pathway ablation for atrioventricular nodal reentrant tachycardia. *J Cardiovasc Electrophysiol* 1993; 4:178-82
29. Janosik DL, Ellenbogen KA: Basic physiology of cardiac pacing and the pacemaker syndrome, *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000; 333-82
30. Donmoyer TL, DeSanctis RW, Austen WG: Experience with implantable pacemakers using myocardial electrodes in the management of heart block. *Ann Thoracic Surg* 1967; 3:218-27

31. Edhag O, Swahn A: Prognosis of patients with complete heart block or arrhythmic syncope who were not treated with artificial pacemakers: A long-term follow-up study of 101 patients. *Acta Med Scand* 1976; 200:457-63
32. Freidberg CK, Donoso E, Stein WG: Nonsurgical acquired heart block. *Ann N Y Acad Sci* 1964; 111:835-47
33. Gadboys HL, Wisoff BG, Litwak RS: Surgical treatment of complete heart block. *JAMA* 1964; 189:97-102
34. Hindman MC, Wagner GS, JaRo M, Atkins JM, Scheinman MM, DeSanctis RW, Hutter AH Jr, Yeatman L, Rubenfire M, Pujura C, Rubin M, Morris JJ: The clinical significance of bundle branch block complicating acute myocardial infarction. 2: Indications for temporary and permanent pacemaker insertion. *Circulation* 1978; 58:689-99
35. Johansson BW: Complete heart block: a clinical, hemodynamic and pharmacological study in patients with and without an artificial pacemaker. *Acta Med Scand Suppl* 1966; 180:1-127
36. Wagner GS: *Marriott's Practical Electrocardiography*, 9th edition. Baltimore, Williams & Wilkins, 1994, p 89
37. DePasquale NP, Bruno MS: Natural history of combined right bundle branch block and left anterior hemiblock (bilateral bundle branch block). *Am J Med* 1973; 54:297-303
38. Dhingra RC, Denes P, Wu D, Chuquimia R, Amat-y-Leon F, Wyndham C, Rosen KM: Syncope in patients with chronic bifascicular block: Significance, causative mechanisms, and clinical implications. *Ann Intern Med* 1974; 81:302-6
39. Kulbertus H, Collignon P: Association of right bundle-branch block with left superior or inferior intraventricular block: Its relation to complete heart block and Adams-Stokes syndrome. *Br Heart J* 1969; 31:435-40
40. Englund A, Bergfeldt L, Rehnqvist N, Astrom H, Rosenqvist M: Diagnostic value of programmed ventricular stimulation in patients with bifascicular block: a prospective study of patients with and without syncope. *J Am Coll Cardiol* 1995; 26:1508-15
41. Twidale N, Heddle WF, Ayres BF, Tonkin AM: Clinical implications of electrophysiology study findings in patients with chronic bifascicular block and syncope. *Aust N Z J Med* 1988; 18:841-7
42. Pastore JO, Yurchak PM, Janis KM, Murphey JD, Zir LM: The risk of advanced heart block in surgical patients with right bundle-branch block and left axis deviation. *Circulation* 1978; 57:677-80
43. Rooney S, Goldiner P, Muss E: Relationship of right bundle branch block and marked left-axis deviation to complete heart block during general anesthesia. *ANESTHESIOLOGY* 1976; 44:64-6
44. McAnulty JH, Rahimtoola SH, Murphy E, DeMots H, Ritzmann L, Kanarek PE, Kauffman S: Natural history of "high-risk" bundle-branch block: final report of a prospective study. *N Engl J Med* 1982; 307:137-43
45. Col JJ, Weinberg SL: The incidence and mortality of intraventricular conduction defects in acute myocardial infarction. *Am J Cardiol* 1972; 29:344-50
46. Domenighetti G, Perret C: Intraventricular conduction disturbances in acute myocardial infarction: Short- and long-term prognosis. *Eur J Cardiol* 1980; 11:51-9
47. Ginks WR, Sutton R, Oh W, Leatham A: Long-term prognosis after acute anterior infarction with atrioventricular block. *Br Heart J* 1977; 39:186-9
48. Ritter WS, Atkins JM, Blomqvist CG, Mullins CB: Permanent pacing in patients with transient trifascicular block during acute myocardial infarction. *Am J Cardiol* 1976; 38:205-8
49. Lamas GA, Muller JE, Turi ZG, Stone PH, Rutherford JD, Jaffe AS, Raabe DS, Rude RE, Mark DB, Califf RM: A simplified method to predict occurrence of complete heart block during acute myocardial infarction. *Am J Cardiol* 1986; 57:1213-9
50. Kusumoto FM, Goldschlager N: Cardiac pacing. *N Engl J Med* 1996; 334:89-97
51. Gammage M, Schofield S, Rankin I, Bennett M, Coles P, Pentecost B: Benefit of single setting rate responsive ventricular pacing compared with fixed rate demand pacing in elderly patients. *PACE* 1991; 14:174-80
52. Rasmussen K: Chronic sinus node disease: Natural course and indications for pacing. *Eur Heart J* 1981; 2:455-9
53. Shah CP, Thakur RK, Xie B, Hoon VK: Implantable cardioverter defibrillators. *Emerg Med Clin North Am* 1998; 16:463-89
54. Andersen HR, Nielsen JC, Thomsen PE, Thuesen L, Mortensen PT, Vestertund T, Pedersen AK: Long-term follow-up of patients from a randomised trial of atrial versus ventricular pacing for sick-sinus syndrome. *Lancet* 1997; 350:1210-6
55. Sra JS, Jazayeri MR, Avitall B, Dhala A, Deshpande S, Blanck Z, Akhtar M: Comparison of cardiac pacing with drug therapy in the treatment of neurocardiogenic (vasovagal) syncope with bradycardia or asystole. *N Engl J Med* 1993; 328:1085-90
56. Benditt DG, Ferguson DW, Grubb BP, Kapoor WN, Kugler J, Lerman BB, Maloney JD, Raviele A, Ross B, Sutton R, Wolk MJ, Wood DL: Tilt table testing for assessing syncope. *American College of Cardiology. J Am Coll Cardiol* 1996; 28:263-75
57. Connolly SJ, Sheldon R, Roberts RS, Gent M: The North American Vasovagal Pacemaker Study (VPS): A randomized trial of permanent cardiac pacing for the prevention of vasovagal syncope. *J Am Coll Cardiol* 1999; 33:16-20
58. Michaelsson M, Riesenfeld T, Jonzon A: Natural history of congenital complete atrioventricular block. *PACE* 1997; 20:2098-101
59. Sholler GF, Walsh EP: Congenital complete heart block in patients without anatomic cardiac defects. *Am Heart J* 1989; 118:1193-8
60. Lillehei CW, Sellers RD, Bonnanbeau RC, Eliot RS: Chronic postsurgical complete heart block with particular reference to prognosis, management, and a new P-wave pacemaker. *J Thorac Cardiovasc Surg* 1963; 46:436-56
61. Kanter RJ, Garson A Jr: Atrial arrhythmias during chronic follow-up of surgery for complex congenital heart disease. *Pacing Clin Electrophysiol* 1997; 20:502-11
62. Gillette PC, Zeigler VL, Case CL, Harold M, Buckles DS: Atrial antitachycardia pacing in children and young adults. *Am Heart J* 1991; 122:844-9
63. Silka MJ, Manwill JR, Kron J, McAnulty JH: Bradycardia-mediated tachyarrhythmias in congenital heart disease and responses to chronic pacing at physiologic rates. *Am J Cardiol* 1990; 65:488-93
64. Kugler JD, Danford DA: Pacemakers in children: An update. *Am Heart J* 1989; 117:665-79
65. Rhodes LA, Walsh EP, Gamble WJ, Triedman JK, Saul JP: Benefits and potential risks of atrial antitachycardia pacing after repair of congenital heart disease. *PACE* 1995; 18:1005-16
66. Eldar M, Griffin JC, Van Hare GF, Witherell C, Bhandari A, Benditt D, Scheinman MM: Combined use of beta-adrenergic blocking agents and long-term cardiac pacing for patients with the long QT syndrome. *J Am Coll Cardiol* 1992; 20:830-7
67. Moss AJ: Clinical management of patients with the long QT syndrome: drugs, devices, and gene-specific therapy. *Pacing Clin Electrophysiol* 1997; 20:2058-60
68. McDonald K, McWilliams E, O'Keefe B, Maurer B: Functional assessment of patients treated with permanent dual chamber pacing as a primary treatment for hypertrophic cardiomyopathy. *Eur Heart J* 1988; 9:893-8
69. Fananapazir L, Cannon RO 3rd, Tripodi D, Panza JA: Impact of dual-chamber permanent pacing in patients with obstructive hypertrophic cardiomyopathy with symptoms refractory to verapamil and beta-adrenergic blocker therapy. *Circulation* 1992; 85:2149-61
70. Fananapazir L, Epstein ND, Curriel RV, Panza JA, Tripodi D, McAreavey D: Long-term results of dual-chamber (DDD) pacing in obstructive hypertrophic cardiomyopathy: Evidence for progressive symptomatic and hemodynamic improvement and reduction of left ventricular hypertrophy. *Circulation* 1994; 90:2731-42
71. Kappenberger L, Linde C, Daubert C, McKenna W, Meisel E, Sadoul N, Chojnowska L, Guize L, Gras D, Jeanrenaud X, Ryden L: Pacing in hypertrophic obstructive cardiomyopathy: A randomized crossover study. *PIC Study Group. Eur Heart J* 1997; 18:1249-56
72. Gadler F, Linde C, Daubert C, McKenna W, Meisel E, Aliot E, Chojnowska L, Guize L, Gras D, Jeanrenaud X, Kappenberger L: Significant improvement of quality of life following atrioventricular synchronous pacing in patients with hypertrophic obstructive cardiomyopathy: Data from 1 year of follow-up. *PIC Study Group. Pacing in Cardiomyopathy. Eur Heart J* 1999; 20:1044-50
73. Linde C, Gadler F, Kappenberger L, Ryden L: Placebo effect of pacemaker implantation in obstructive hypertrophic cardiomyopathy. *PIC Study Group. Pacing in Cardiomyopathy. Am J Cardiol* 1999; 83:903-7
74. Maron BJ, Nishimura RA, McKenna WJ, Rakowski H, Josephson ME, Kievall RS: Assessment of permanent dual-chamber pacing as a treatment for drug-refractory symptomatic patients with obstructive hypertrophic cardiomyopathy: A randomized, double-blind, crossover study (M-PATHY). *Circulation* 1999; 99:2927-33
75. Nishimura RA, Symanski JD, Hurrell DG, Trusty JM, Hayes DL, Tajik AJ: Dual-chamber pacing for cardiomyopathies: A 1996 clinical perspective. *Mayo Clin Proc* 1996; 71:1077-87
76. Auricchio A, Sommariva L, Salo RW, Scafuri A, Chiariello L: Improvement of cardiac function in patients with severe congestive heart failure and coronary artery disease by dual chamber pacing with shortened AV delay. *PACE* 1993; 16:2034-43
77. Hochleitner M, Hortnagl H, Fridrich L, Gschnitzer F: Long-term efficacy of physiologic dual-chamber pacing in the treatment of end-stage idiopathic dilated cardiomyopathy. *Am J Cardiol* 1992; 70:1320-5
78. Linde C, Gadler F, Edner M, Nordlander R, Rosenqvist M, Ryden L: Results of atrioventricular synchronous pacing with optimized delay in patients with severe congestive heart failure. *Am J Cardiol* 1995; 75:919-23
79. Nishimura RA, Hayes DL, Holmes DR Jr, Tajik AJ: Mechanism of hemodynamic improvement by dual-chamber pacing for severe left ventricular dysfunction: An acute Doppler and catheterization hemodynamic study. *J Am Coll Cardiol* 1995; 25:281-8
80. Leclercq C, Cazeau S, Le Breton H, Ritter P, Mabo P, Gras D, Pavin D, Lazarus A, Daubert JC: Acute hemodynamic effects of biventricular DDD pacing in patients with end-stage heart failure. *J Am Coll Cardiol* 1998; 32:1825-31
81. Heinz G, Kratochwill C, Koller-Strametz J, Kreiner G, Grimm M, Grabenwoger M, Laufer G, Gossinger H: Benign prognosis of early sinus node dysfunction after orthotopic cardiac transplantation. *PACE* 1998; 21:422-9
82. Kratochwill C, Schmid S, Koller-Strametz J, Kreiner G, Grabenwoger M, Grimm M, Laufer G, Heinz G: Decrease in pacemaker incidence after orthotopic heart transplantation. *Am J Cardiol* 1996; 77:779-83
83. Balaji S, Johnson TB, Sade RM, Case CL, Gillette PC: Management of atrial flutter after the Fontan procedure. *J Am Coll Cardiol* 1994; 23:1209-15
84. Saksena S, Epstein AE, Lazzara R, Maloney JD, Zipes DP, Benditt DG, Camm

- AJ, Domanski MJ, Fisher JD, Gersh BJ: NASPE/ACC/AHA/ESC medical/scientific statement special report: Clinical investigation of antiarrhythmic devices: a statement for healthcare professionals from a Joint Task Force of the North American Society of Pacing and Electrophysiology, the American College of Cardiology, the American Heart Association, and the Working Groups on Arrhythmias and Cardiac Pacing of the European Society of Cardiology. *PACE* 1995; 18:637-54
85. Attuel P, Pellerin D, Mugica J, Coumel P: DDD pacing: An effective treatment modality for recurrent atrial arrhythmias. *PACE* 1988; 11:1647-54
86. Fitts SM, Hill MR, Mehra R, Friedman P, Hammill S, Kay GN, Prakash A, Webb C, Saksena S: Design and implementation of the Dual Site Atrial Pacing to Prevent Atrial Fibrillation (DAPPAF) clinical trial. DAPPAF Phase 1 Investigators. *J Interv Cardiac Electrophysiol* 1998; 2:139-44
87. Saksena S, Prakash A, Hill M, Krol RB, Munsif AN, Mathew PP, Mehra R: Prevention of recurrent atrial fibrillation with chronic dual-site right atrial pacing. *J Am Coll Cardiol* 1996; 28:687-94
88. Saksena S: Pacing therapy for atrial fibrillation. *Thorac Cardiovasc Surg* 1999; 47:339-41
89. Daoud EG, Timmermans C, Fellows C, Hoyt R, Lemery R, Dawson K, Ayers GM: Initial clinical experience with ambulatory use of an implantable atrial defibrillator for conversion of atrial fibrillation. *Metrix Investigators. Circulation* 2000; 102:1407-13
90. Jung W, Wolpert C, Smaizadeh B, Spehl S, Herwig S, Schumacher B, Lewalter T, Omran H, Schimpf R, Vahlhaus C, Welz A, Luderitz B: Clinical experience with implantable atrial and combined atrioventricular defibrillators. *J Interv Cardiac Electrophysiol* 2000; 4:185-95
91. Saksena S: The impact of implantable cardioverter defibrillator therapy on health care systems. *Am Heart J* 1994; 127:1193-200
92. Zipes DP, Roberts D: Results of the international study of the implantable pacemaker cardioverter-defibrillator: A comparison of epicardial and endocardial lead systems. The Pacemaker-Cardioverter-Defibrillator Investigators. *Circulation* 1995; 92:59-65
93. Wood MA, Stambler BS, Damiano RJ, Greenway P, Ellenbogen KA: Lessons learned from data logging in a multicenter clinical trial using a late-generation implantable cardioverter-defibrillator. The Guardian ATP 4210 Multicenter Investigators Group. *J Am Coll Cardiol* 1994; 24:1692-9
94. Bocker D, Block M, Isbruch F, Wietholt D, Hammel D, Borggrefe M, Breithardt G: Do patients with an implantable defibrillator live longer? *J Am Coll Cardiol* 1993; 21:1638-44
95. Bocker D, Block M, Isbruch F, Fastenrath C, Castrucci M, Hammel D, Scheld HH, Borggrefe M, Breithardt G: Benefits of treatment with implantable cardioverter-defibrillators in patients with stable ventricular tachycardia without cardiac arrest. *Br Heart J* 1995; 73:158-63
96. Grimm W, Flores BF, Marchlinski FE: Symptoms and electrocardiographically documented rhythm preceding spontaneous shocks in patients with implantable cardioverter-defibrillator. *Am J Cardiol* 1993; 71:1415-8
97. Hook BG, Marchlinski FE: Value of ventricular electrogram recordings in the diagnosis of arrhythmias precipitating electrical device shock therapy. *J Am Coll Cardiol* 1991; 17:985-90
98. Kim SG, Maloney JD, Pinski SL, Choue CW, Ferrick KJ, Roth JA, Gross J, Brodman R, Furman S, Fisher JD: Influence of left ventricular function on survival and mode of death after implantable defibrillator therapy (Cleveland Clinic Foundation and Montefiore Medical Center experience). *Am J Cardiol* 1993; 72:1263-7
99. Mehta D, Saksena S, Krol RB: Survival of implantable cardioverter-defibrillator recipients: Role of left ventricular function and its relationship to device use. *Am Heart J* 1992; 124:1608-14
100. The Antiarrhythmic versus Implantable Defibrillators (AVID) Investigators: A comparison of antiarrhythmic-drug therapy with implantable defibrillators in patients resuscitated from near-fatal ventricular arrhythmias. The Antiarrhythmics versus Implantable Defibrillators (AVID) Investigators. *N Engl J Med* 1997; 337:1576-83
101. CASCADE Investigators: Cardiac arrest in Seattle: Conventional versus amiodarone drug evaluation (the CASCADE study). *Am J Cardiol* 1991; 67:578-84
102. Mason JW: A comparison of seven antiarrhythmic drugs in patients with ventricular tachyarrhythmias. Electrophysiologic Study versus Electrocardiographic Monitoring Investigators. *N Engl J Med* 1993; 329:452-8
103. A randomized trial of propranolol in patients with acute myocardial infarction. I: Mortality results. *JAMA* 1982; 247:1707-14
104. Yusuf S, Peto R, Lewis J, Collins R, Sleight P: Beta blockade during and after myocardial infarction: an overview of the randomized trials. *Prog Cardiovasc Dis* 1985; 27:335-71
105. Borggrefe M, Chen X, Martinez-Rubio A, Hindricks G, Haverkamp W, Block M, Breithardt G: The role of implantable cardioverter defibrillators in dilated cardiomyopathy. *Am Heart J* 1994; 127:1145-50
106. Saksena S, Gielchinsky I, Tullo NG: Argon laser ablation of malignant ventricular tachycardia associated with coronary artery disease. *Am J Cardiol* 1989; 64:1298-304
107. Svenson RH, Littmann L, Gallagher JJ, Selle JG, Zimmern SH, Fedor JM, Colavita PG: Termination of ventricular tachycardia with epicardial laser photo-coagulation: A clinical comparison with patients undergoing successful endocardial photo-coagulation alone. *J Am Coll Cardiol* 1990; 15:163-70
108. Blanck Z, Dhala A, Deshpande S, Sra J, Jazayeri M, Akhtar M: Bundle branch reentrant ventricular tachycardia: Cumulative experience in 48 patients. *J Cardiovasc Electrophysiol* 1993; 4:253-62
109. Klein LS, Shih HT, Hackett FK, Zipes DP, Miles WM: Radiofrequency catheter ablation of ventricular tachycardia in patients without structural heart disease. *Circulation* 1992; 85:1666-74
110. Leclercq JF, Chouty F, Cauchemez B, Leenhardt A, Coumel P, Slama R: Results of electrical fulguration in arrhythmogenic right ventricular disease. *Am J Cardiol* 1988; 62:220-4
111. Groh WJ, Silka MJ, Oliver RP, Halperin BD, McAnulty JH, Kron J: Use of implantable cardioverter-defibrillators in the congenital long QT syndrome. *Am J Cardiol* 1996; 78:703-6
112. Moss AJ, Hall WJ, Cannom DS, Daubert JP, Higgins SL, Klein H, Levine JH, Saksena S, Waldo AL, Wilber D, Brown MW, Heo M: Improved survival with an implanted defibrillator in patients with coronary disease at high risk for ventricular arrhythmia. Multicenter Automatic Defibrillator Implantation Trial Investigators. *N Engl J Med* 1996; 335:1933-40
113. Belhassen B, Viskin S, Fish R, Glick A, Setbon I, Eldar M: Effects of electrophysiologic-guided therapy with Class IA antiarrhythmic drugs on the long-term outcome of patients with idiopathic ventricular fibrillation with or without the Brugada syndrome. *J Cardiovasc Electrophysiol* 1999; 10:1301-12
114. Brugada J, Brugada R, Brugada P: Right bundle-branch block and ST-segment elevation in leads V1 through V3: A marker for sudden death in patients without demonstrable structural heart disease. *Circulation* 1998; 97:457-60
115. Gussak I, Antzelevitch C, Bjerregaard P, Towbin JA, Chaitman BR: The Brugada syndrome: Clinical, electrophysiologic and genetic aspects. *J Am Coll Cardiol* 1999; 33:5-15
116. Maron BK, Win-Kuang S, Link MS, Epstein AE, Almquist AK, Daubert JP, Bardy GH, Favale S, Rea RF, Boriani G, Estes III M, Spirito P: Efficacy of implantable cardioverter-defibrillators for the prevention of sudden cardiac death in patients with hypertrophic cardiomyopathy. *N Engl J Med* 2000; 342:365-73
117. Link MS, Wang PJ, Haugh CJ, Homoud MK, Foote CB, Costeas XB, Estes NA III: Arrhythmogenic right ventricular dysplasia: Clinical results with implantable cardioverter defibrillators. *J Interv Cardiac Electrophysiol* 1997; 1:41-8
118. Silka MJ, Kron J, Dunnigan A, Dick MD: Sudden cardiac death and the use of implantable cardioverter-defibrillators in pediatric patients. The Pediatric Electrophysiology Society. *Circulation* 1993; 87:800-7
119. Glikson M, Espinosa RE, Hayes DL: Expanding indications for permanent pacemakers. *Ann Intern Med* 1995; 123:443-51
120. Mushlin AI, Hall WJ, Zwanziger J, Gajary E, Andrews M, Marron R, Zou KH, Moss AJ: The cost-effectiveness of automatic implantable cardiac defibrillators: Results from MADIT. Multicenter Automatic Defibrillator Implantation Trial. *Circulation* 1998; 97:2129-35
121. Bigger JT Jr, Whang W, Rottman JN, Kleiger RE, Gottlieb CD, Namerow PB, Steinman RC, Estes NA III: Mechanisms of death in the CABG Patch trial: A randomized trial of implantable cardiac defibrillator prophylaxis in patients at high risk of death after coronary artery bypass graft surgery. *Circulation* 1999; 99:1416-21
122. Lorga-Filho A, Geelen P, Vanderheyden M, Malacki T, Primo J, Goethals M, Wellens F, Brugada P: Early benefit of implantable cardioverter defibrillator therapy in patients waiting for cardiac transplantation. *PACE* 1998; 21:1747-50
123. Schmidinger H: The implantable cardioverter defibrillator as a "bridge to transplant": A viable clinical strategy? *Am J Cardiol* 1999; 83:151D-7D
124. Leung S-K, Lau C-P, Camm AJ: An overview of sensors: Ideal characteristics, sensor combination, and automaticity. *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 219-48
125. Nappholz T, Kay GN: Rate-adaptive pacing based on impedance-derived minute ventilation. *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 271-92
126. Boute W, Feith F, Leung S-K, Lau C-P: Evoked QT interval-based and intracardiac impedance-based pacemakers. *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 293-306
127. Toivonen L, Lommi J: Dependence of atrial sensing function on posture in a single-lead atrial triggered ventricular (VDD) pacemaker. *PACE* 1996; 19:309-13
128. Sun ZH, Stjernvall J, Laine P, Toivonen L: Extensive variation in the signal amplitude of the atrial floating VDD pacing electrode. *PACE* 1998; 21:1760-5
129. Naegeli B, Straumann E, Gerber A, Schuiki E, Kunz M, Niederhauser U, Bertel O: Dual chamber pacing with a single-lead DDD pacing system. *PACE* 1999; 22:1013-9
130. Israel CW, Kruse IM, Van Mechelen R, Kroes G, Heynen H, Lokhoff N: Results from the use of a preshaped lead for single-pass VDD/DDD stimulation. *PACE* 1999; 22:1314-20
131. Barold SS: Timing cycles and operational characteristics of pacemakers. *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 727-825
132. Schmidt JA, Stotts LJ: Bipolar pacemaker leads: New materials, new technology. *J Invest Surg* 1998; 11:75-81
133. de Voogt WG: Pacemaker leads: performance and progress. *Am J Cardiol* 1999; 83:187D-91D

134. Pinski SL, Fahy GJ: The proarrhythmic potential of implantable cardioverter-defibrillators. *Circulation* 1995; 92:1651-64
135. Schaumann A, von zur Muhlen F, Herse B, Gonska BD, Kreuzer H: Empirical versus tested antitachycardia pacing in implantable cardioverter defibrillators: A prospective study including 200 patients. *Circulation* 1998; 97:66-74
136. Raitt MH, Dolack GL, Kudenchuk PJ, Poole JE, Bardy GH: Ventricular arrhythmias detected after transvenous defibrillator implantation in patients with a clinical history of only ventricular fibrillation: Implications for use of implantable defibrillator. *Circulation* 1995; 91:1996-2001
137. Bernstein AD, Camm AJ, Fletcher RD, Gold RD, Rickards AF, Smyth NP, Spielman SR, Sutton R: The NASPE/BPEG generic pacemaker code for antibradyarrhythmia and adaptive-rate pacing and antitachyarrhythmia devices. *PACE* 1987; 10:794-9
138. Warren JA, Nelson JP: Pacemaker and ICD pulse generator circuitry, *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2000, pp 194-216
139. Wood MA: Sensing and arrhythmia detection by implantable devices, *Clinical Cardiac Pacing and Defibrillation*, 2nd edition. Edited by Ellenbogen KA, Kay GN, Wilkoff BL. Philadelphia, WB Saunders, 2001, pp 68-126
140. Saksena S, An H, Mehra R, DeGroot P, Krol RB, Burkhardt E, Mehta D, John T: Prospective comparison of biphasic and monophasic shocks for implantable cardioverter-defibrillators using endocardial leads. *Am J Cardiol* 1992; 70:304-10
141. Jung W, Manz M, Moosdorf R, Spehl S, Wolpert C, Korte T, Luderitz B: Clinical efficacy of shock waveforms and lead configurations for defibrillation. *Am Heart J* 1994; 127:985-93
142. Olsovsky MR, Hodgson DM, Shorofsky SR, Kavesh NG, Gold MR: Effect of biphasic waveforms on transvenous defibrillation thresholds in patients with coronary artery disease. *Am J Cardiol* 1997; 80:1098-100
143. Nunain SO, Roelke M, Trouton T, Osswald S, Kim YH, Sosa-Suarez G, Brooks DR, McGovern B, Guy M, Torchiana DF: Limitations and late complications of third-generation automatic cardioverter-defibrillators. *Circulation* 1995; 91:2204-13
144. Nair M, Saoudi N, Kroiss D, Letac B: Automatic arrhythmia identification using analysis of the atrioventricular association. Application to a new generation of implantable defibrillators. Participating Centers of the Automatic Recognition of Arrhythmia Study Group. *Circulation* 1997; 95:967-73
145. Almendral J, Arenal A, Villacastin JP, San Roman D, Bueno H, Alday JM, Pastor A, Delcan JL: The importance of antitachycardia pacing for patients presenting with ventricular tachycardia. *PACE* 1993; 16:535-9
146. The PCD Investigators: Clinical outcome of patients with malignant ventricular tachyarrhythmias and a multiprogrammable implantable cardioverter-defibrillator implanted with or without thoracotomy: An international multicenter study. *J Am Coll Cardiol* 1994; 23:1521-30
147. Porterfield JG, Porterfield LM, Smith BA, Bray L, Voshage L, Martinez A: Conversion rates of induced versus spontaneous ventricular tachycardia by a third generation cardioverter defibrillator. The VENTAK PRx Phase I Investigators. *PACE* 1993; 16:170-3
148. Gross JN, Sackstein RD, Song SL, Chang CJ, Kawinishi DT, Furman S: The antitachycardia pacing ICD: Impact on patient selection and outcome. *PACE* 1993; 16:165-9
149. Bardy GH, Poole JE, Kudenchuk PJ, Dolack GL, Kelso D, Mitchell R: A prospective randomized repeat-crossover comparison of antitachycardia pacing with low-energy cardioversion. *Circulation* 1993; 87:1889-96
150. Geelen P, Lorga Filho A, Chauvin M, Wellens F, Brugada P: The value of DDD pacing in patients with an implantable cardioverter defibrillator. *PACE* 1997; 20:177-81
151. Best PJ, Hayes DL, Stanton MS: The potential usage of dual chamber pacing in patients with implantable cardioverter defibrillators. *PACE* 1999; 22:79-85
152. Higgins SL, Williams SK, Pak JP, Meyer DB: Indications for implantation of a dual-chamber pacemaker combined with an implantable cardioverter-defibrillator. *Am J Cardiol* 1998; 81:1360-2